

Review

Induced Pluripotent Stem Cells (IpsCs) Based Liver Organoid: the Benefits and Challenges

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Key Words

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Abstract

The liver is the main metabolic organ and functions to regulate many physiological functions in the human body. Approximately 70% of liver mass consists of hepatic cells (hepatocytes), which execute the liver's metabolic processes. When liver damage progresses to a chronic condition, such as end-stage liver disease (ESLD) or cirrhosis of the liver, the patient's only option for therapy is organ transplantation if the supply of available transplanted organs is insufficient to meet the patient's needs. The fundamental objective of the search for alternatives to organ transplantation has been to make liver tissue replacement more accessible and to produce hepatic and bioartificial liver tissue. Multiple hepatic cell lineages can be formed from human-induced pluripotent stem cells (hiPSCs) from embryoid bodies to become mature hepatocytes. hiPSCs also show a promising source for manufacturing human liver spheroids and are made to produce three-dimensional hepatobiliary organoids, and in some ways, it also briefly highlights important features of early hepatogenesis. Unquestionably, the art of cell culture has evolved to include the use of organoid technology as a resource for learning human biology in the context of health and illness. Organoids are essentially miniature organs that can grow in a three-dimensional matrix to resemble genuine organs in terms of both structure and function. This review summarized alternative protocols to differentiate hepatocytes from iPSC and to produce liver organoids based on iPSC in various ways. The growth of human iPSCs into liver organoids has been accomplished using several procedures.

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Introduction

The liver, the primary metabolic organ, controls various physiological processes in the human body [1]. Approximately 70% of liver mass comprises hepatic cells (hepatocytes), which perform metabolic tasks for the liver, including chemical detoxification, plasma protein synthesis, regulation of amino acids and carbs, and the induction of inflammatory and immunological responses. The sole therapeutic option for a patient whose liver has been

damaged and has developed into a chronic condition such as end-stage liver disease (ESLD) or cirrhosis of the liver is organ transplantation [1]. Unfortunately, when it reaches its final stage, the damage to liver function is irreversible at this point, so decompensation will occur in different organs and organ systems, including lung tissue, which can result in bleeding varicose, renal damage, and ascites [2].

Increased survival rates may result from the transplantation of patients with stages 2 and 3 acute liver failure. Although more patients are being held [3], the number of those waiting for transplants continues to increase, and the supply of available transplanted organs cannot keep up with demand [4]. Expanding the availability of liver tissue replacement and creating hepatic and bioartificial liver tissue have been the main goals of the search for alternatives to whole organ transplantation [5]. Organoid culture can recreate the physiological and pathological circumstances of the tissue while preserving the DNA contained in autologous tissue [6].

Advances in regenerative medicine are opening new insights and new hope in the therapy of irreversible liver damage. Regenerative medicine for the liver focuses particularly on the development of new therapies that functionally reverse damage to existing liver tissue or create an entirely new organ. The advancement of liver regenerative medicine has benefited from the understanding of cellular and molecular principles relating to organogenesis and regeneration over the past few decades. Regenerative medicine, when compared to current operational therapy; therefore, it is less intrusive, less expensive, and a solution to donor limits, immunological rejection, and other issues. The ideal treatment for liver cirrhosis is liver regeneration therapy [7].

The latest technologies in cellular and molecular research are rapidly developing to meet the needs of clinical applications that involve the diagnosis and treatment of liver disease.

[8] Several recent studies found that the notion of co-culturing induced pluripotent stem cells with diverse nonparenchymal cell supporting cells can acquire higher differentiation and develop and boost the function of hepatocyte cells produced [9]. In this approach, some researchers employ bioengineering to construct liver organoids derived from a decellularized liver [10].

Human-induced pluripotent stem cells' ability to differentiate into several hepatic cell lineages

For several years, scientists have worked to promote the three main lineages of the germ layers *in vitro* development from basic, possibly pluripotent cells. During embryological development, to recreate the necessary molecular and cellular signaling, the traditional strategy for building protocols that imitate patterns and phases was employed. Most important protocol either use one of the numerous cellular aggregation techniques or encourage the cultural differentiation as a monolayer when dealing with pluripotent cells. It is possible that over time, in what seems to be a random process, EB develops the regional differentiation. One strategy involves using various techniques, such as transplanting three-dimensional (3D) gel constructs made of Matrigel into immunodeficient animals and combining them with other cells to create an endoderm that is steered to the liver. One of these two small molecules causes enhanced adult marker expression and functional activity, including cytochrome P450s, whereas the other reduces the fetal marker expression [11].

Different development procedures, including those for hepatocytes made from human iPSCs, have been created. For this stage, an essential prerequisite is to use Activin A for the initial induction of definitive endoderm (DE). In the hepatic specification and throughout various stages of protocol development, culture media, and extra growth factors are also used as additional components. The results show that different techniques of differentiation have varying degrees of success; for instance, after 16–25 days of human iPSC hepatic

differentiation, positive adult hepatocyte cells can be identified by the presence of albumin or Alpha 1 antitrypsin [7]. Brief exposure to the factor Wnt3a, which is expressed at the human heart's developmental stage and interacts specifically with activin A, can increase DE and hepatic output. At a later stage of embryonic development, fibroblast growth factors 2 (FGF2) work in conjunction with bone morphogenic protein-4 (BMP4) to aid in the production of DE cells. Another important finding is that in the presence of serum from cow fetuses in culture media, the effects of all the factors that stimulate the development of early mammals are inhibited. This approach will produce functionally enhanced hepatocyte-like cells. Different marker genes expressed out of DE during embryonic development include SRY, Sox17, and Foxa2 [7, 12].

The next step toward hepatocyte formation is the induction from DE of the development of liver progenitor cells or hepatoblasts. In cell culture, induction is accomplished by introducing a certain growth factor, with hepatocyte growth factor (HGF) serving as the primary one. During the liver development process, hepatocyte nuclear factor 4 alpha (HNF4 α) expression will increase and mark differentiation toward the hepatocyte line during *in vitro* differentiation. The essential marker of the liver progenitor cells is the α -fetoprotein (AFP) serum glycoprotein, which is expressed by primordial hepatocytes [7].

The last step in the differentiation process is induced by hepatocyte maturation. This was obtained in cell culture by adding Oncostatin M (OSM), which in combination with glucocorticoids is a cytokine from the interleukin-6 family to cell culture media. Morphological observations such as hepatocytes and intracellular glycogen production are consistent with a cell-like differentiation of the hepatocytes. Strategies to change the cells of the line of descent from hepatoblasts or hepatocytes on a fetus into a cell with characteristics of adult primary hepatocytes [7].

The efficiency of differentiation for each type of cell phase was measured using the hepatic stage-specific marker, with the results obtained being efficiencies reliably greater than 90% (up to 98%) for the second phase of the cell endoderm and the definitive progenitor liver but more variable (between 50% and 90%) for the final phase, that is, in adult cells such as hepatic cells [7]. Variations in culture conditions, including cell culture, density before and after the induction of endoderm, and a selection of essential growth agents and substances, can significantly affect each differentiation stage's efficacy. Examples include the size of iPSC colonies that are not differentiated at the time of differentiation initiation, iPSC colony culture, and cell culture [7, 12-14].

In 3D co-culture, the main hepatocytes and the epithelial sinusoidal liver cells assist each other. The concept has been extended to the hepatocyte-like cells derived from the iPSC, which shows that the co-cultured endothelial cells and stromal support the maturation of cells such as hepatocytes by touch cells or by paracrine factor. Specific DE hepatocytes have recently been cultured with human umbilical vein endothelial cells and mesenchymal stem cells (MSCs), which can produce 3D cell clusters in which iPSC-derived cells express genes that connect to other hepatocytes, such as AFP and albumin, suggesting that cluster formation may speed up hepatocyte maturation [15].

There has been a lot of use of hepatocyte reference controls such as cell lines or cultured hepatocytes and a population standard that can be replicated, but these lines do not represent the proper physiological level of the particular function of hepatocytes. Therefore, primary human hepatocytes cryopreserved, are freshly isolated, or are not cultured are usually considered ideal reference controls. Although all work quickly degrades after being stored in traditional culture systems, certain functional research calls for cells to be cultivated for several hours to days. These studies include those involving morphology, phenotypes, and primary human hepatocytes [16].

Based on the work of Ma et al. that has been conducted, there are studies on the efficient differentiation of iPSC against homogeneous functional hepatocyte populations [17]. Factors of liver transcription, such as HNF3 β , GATA4, C/EBP α , C/EBP β , and BMP signaling (BMP-2 and BMP-4) have significant involvement in the differentiation of hepatocytes and the development of the liver. These factors were expressed throughout differentiation, which was a key element in improving the ability of these cells to differentiate into hepatocytes later on.

[18] A particular group of liver genes, including albumin, 1-AT, tyrosine aminotransferase, and G-6-P, which are more mature indicators of hepatocytes and have significant roles in the liver, will be expressed by human iPSC-derived hepatocytes (hiHs). Besides functional testing, hiHs exhibit glycogen accumulation, indocyanine green (ICG) absorption and excretion, and albumin secretion into the medium. These results suggest that the time needed for hiHs to produce albumin at a level comparable to that of hESC-derived hepatocytes (20–22 days) is longer (26–27 days after differentiation). It represents the initial difference in hESC–hiPSC differentiation [18, 19].

There are vast variations in liver differentiation protocols, diagnostic methods, and phenotypic or functional outcomes. Hence, comparing the effectiveness of the pluripotent stem cell pathways to produce functional hepatocytes precisely is challenging. The hiPSC line, as a general observation, presents differentiation and performance of the hepatocytes more varied than the ESC line, specifically the H9 line. This is because the available protocol differentiation has been developed to track the ESC, and the protocol is not intended to discuss potential memory epigenetics that are maintained or irregularities that may be owned by the iPSC track, ensuring that the iPSC path responds to weak heart differentiation signals [20, 21].

How can organoids research benefit end-stage liver disease?

Heaps of the current research is behind the successful advances in medical treatment using cancer cell or animal cell models, both of which have drawbacks, especially concerning medical applications. Nevertheless, the development of stem cell biology has been able to culture tissues that resemble the liver and intestines over a long period from local tissue or pluripotent stem cells [15]. Three-dimensional structures, called organoids, represent important structures and complexity of function beyond the frequent and changing traditional *in vitro* cell culture models [22].

Both the ideal immunosuppressive protocols and the most effective cellular combination that may engraft and multiply over an extended period must be properly identified. Numerous studies demonstrated that diverse cell types can be created from induced pluripotent stem cells (iPSCs), including hepatocytes, cholangiocytes, endothelial cells, and Kupffer cells, which are all found in the liver. The development of useful bioartificial livers has been facilitated by the growing interest in the study of 3D organoids that self-assemble or are driven by matrices [23]. The various cell types that make up the liver should be present in a realistic liver replica, and the spatial arrangement of these cells should resemble that of the tissue architecture [24].

The liver was successfully encapsulated into alginate material and it survived and functioned well when transplanted into immunocompetent mice. Better cell models and creating transplantable human tissue are prerequisites for establishing a renewable source of liver tissue [25]. The manufacture of human embryonic hESCs offers fascinating opportunities for the advancement of biology, models for diseases, and cell treatment [26]. Significant progress toward achieving this goal is hampered by the dependence on the ingredients used of animal origin (e.g., Matrigel), immortal cell lines, and their resulting forms that are difficult to control and reproduce [27].

Presently, organoid technology has developed into an art in cell culture to study human biology in the world of health and certain diseases. Generally, organoids can simply be said to be mini-structures of organs in a 3D form that can develop into a 3D matrix in which the aspects of the structure and function are the same as the real organs. Organoids have been extensively exploited as brand-new therapeutic candidates for things such as illness modeling and medication discovery [2]. Exogenous factors promote cell self-renewal, proliferation, and differentiation via inducing several signaling pathways and support tissue-specific organogenesis, all of which contribute to the production of organoids [28]. Producing liver organoids using bioengineering can produce more physiologically realistic and biomedically useful liver organoids [29].

Disease models in the form of organoids have been developed substantially, such as acquired disorders connected to toxin products that have an organoid model and hereditary high cholesterol has been better defined; this has allowed for greater knowledge and research of already prescribed medications as well as the identification of new medications [2]. The diversity of functions performed by the human liver, the usefulness of liver organoids in the modeling of many liver illnesses, and the possibility of using liver organoids as cell-based therapies in regenerative medicine make them of particular interest. Organoid models also open up new avenues for personalized medicine and drug development because they may be created from patient tissues [30]. An important turning point in the modeling of liver illness is the use of liver organoids, which transcend the limitations of bidimensional culture and the high expense of *in vivo* models [31]. Access to multicellular organotypic surrogate models for illness, toxicity, and drug development would be considerably enhanced with interactions and architecture that are similar to those *in vivo*. Organoids and microfluidic chip technologies would be combined in this, potentially leading to new therapeutic strategies [32].

Human-induced pluripotent stem cell-based 3D liver organoid production

Organoids are a 3D culture system that uses adult stem cells and their offspring to develop and represent the physiological state of the cell under *in vivo* conditions [3]. The formation of liver organoids from iPSC was first introduced by Takebe et al. using co-culture. In his model, human MSCs and human umbilical vein endothelial cells were co-cultured with liver progenitor cells that were produced through the progressive differentiation of iPSC in two-dimensional (2D) cell cultures (HUVECs). Then, on a microscope, iPSC-liver buds (LB), which spontaneously formed on culture in Matrigel, were visible. Additionally, the presence of a connection to the host vessel at the moment of transplant makes the human blood vessel structure in the iPSC-LB functional. Particularly, albumin secretion into blood arteries by liver cells implanted in LB started from days 10 to 45 after transplantation in mice. The bud organs' structure, which shows regenerating powers and prevents death from liver failure, is more significant [33].

The primary objective anticipated by the researchers is to produce functional liver organoids by combining current techniques with the advancement of bioengineering technology. The development of "organs-on-a-chip," bioengineered miniature organs relies on exact manipulation of the environment for hepatocyte function. Frequently, mature hepatocytes derived directly from humans are used in this approach. The chip's ability to mechanically manage the spatiotemporal interactions of the various cell types is made possible by the incorporation of many cell types. Microfluidics and soft lithography technology have created the culture environment, which frequently results in a static culture environment. The precise regulation of input (drugs, nutrients, and oxygen) and output (metabolites, biosensing, and electrical potential) made possible by combining technology and bioengineering will have many benefits and improve liver function. A mix of extracellular signals that are inductive and repressive at different concentrations determines the fate of the human liver [7, 34, 35].

The generated hepatocyte-like cells have unique secretory properties (albumin and urea) and drug-metabolizing capabilities. They can also absorb ICG and store lipids and glycogen (CYP3A4 activity); the system's biliary structure demonstrates gamma-glutamyltransferase activity, the ability to release rhodamine, and the capacity to store bile acids [36].

Mesenchymal stromal cell and iPSC-derived endothelial cell liver organoids exhibit considerable albumin expression and production, elevated CYP1A1, CYP1A2, and TDO2 expression, and decreased TGF-beta and Wnt signaling activity. Large changes in protein expression caused by a particular combination of nonparenchymal cells were discovered by proteomic analysis to be connected to integrin profiles and TGF-beta/Wnt signaling activity [37, 38].

Hepatocytes, liver sinusoidal endothelial cells, and MSCs are a mixture of human cells that, when cultivated *in vitro* on a thick layer of Matrigel TM, self-regulate to create structures that mimic liver organoids in 24 h. After being cultivated for up to 10 days in a bioreactor, these liver organoids display different functional characteristics such as hepatic parenchymal cells, the activity of cytochromes P450, CYP3A4, CYP2B6, and CYP2C9, and mRNA expression on multiple marker genes and other enzymes [38].

Three-dimensional culture systems and liver organoids

An interesting approach to long-term 3D cell culture is a technique introduced in the late 1990s. A technique created by Broutier et al. produces organoid livers using EpCam and ductal cells from human livers that are either healthy or injured. It can develop into a 3D structure with progenitor biliary cells that enable them to differentiate into liver lineages when cultured in Matrigel or using a low attachment plate with EGF, HGF, FGF, and RSP01. The benefit of this technique over iPSC-derived organoids is that these organoids may be cryopreserved and cultivated for an extended period of time (up to more than a year) while maintaining genetic stability. This facilitates the cell banking procedure [39].

Invagination of the 3D culture of pluripotent stem cells of human origin, along with a continuous and dynamic pattern of structural morphogenesis of the liver, biliary, and pancreatic, was described by Koike et al. In the absence of external stimuli, retinoic acid-dependent formation of hepatobiliary-pancreatic organ domains designated at the foregut-midgut boundary organoids is enabled by the interaction between anterior and posterior gut spheroids produced from pluripotent stem cells of human origin [40].

Akbari et al. developed and characterized hepatic organoids (eHEPO) that can be produced in 2 weeks and multiplied over more than 16 months without losing the capacity to become mature hepatocytes. Table 1-4 show the various culture methods with the combination of cells used and the medium and supplementation used to produce a functional organoid liver in the last 3 years. From these tables, we can see that the generation of the organoid liver can be produced with various technologies and requires various supplements [41].

Comparison between 2D and 3D organoid

The genetic landscape and histoarchitecture could not be represented by cells cultivated in two dimensions. Researchers have been successful in creating culture conditions for the organoid system to produce a better model that can imitate the histoarchitecture and genetic landscape of liver cancer. Organoids are characterized by self-structuring 3D structures that respond to the original architecture of the organ and/or tumor in the *in vivo* state and can be constructed from multiple sources. Organoids can currently be created from adult stem cells that are unique to a particular organ, as well as from embryonic or induced pluripotent stem cells, tumor cells, or adult stem cells (referred to as tumoroids) [3].

Table 1. Various methods to generate liver organoid from iPSC

No	Author	Year	Cell source	Product	Methods	Functional indicator/marker	Result	Reference
1	Yuan Guan et al	2017	iPSc	Modeling ALGS liver pathology.	The endodermal spheres then developed posterior foregut-like structures on a Matrigel scaffold in low concentration.	ADH, GSRA1, CYP3A4, TTR, TDO2, GSTA1, and FAH. CK8, HNF4A, CK19, EpCAM, and SOX9	(iPSCs) undergo stages of differentiation that replicate the human liver's embryonic development	[42]
2	Soon seng et al	2018	iPSc	Liver organoid	Hepatic progenitors (IH) generated from iPSC created organoids most effectively in ICC scaffolds that mimicked liver bud formation.	Human albumin, immunohistokimia, cytochrome p450 isoform (CYP3A4, CYP2C9), hepatic polarity protein for bile canaliculi, bile salt efflux (cholyl-lysyl-fluorescence)	The resulting organoids could integrate, vascularize, and function after being implanted into the livers of immune-deficient mice -PGECS that can be stored up to 1021 cells in size	[27]
3	Ran-ran Zhang	2018	iPSc cell lines	CDX2+ posterior gut endoderm cells (PGECS) derived liver bud	To specify PGECS, the produced DE cells were then replated at a 1:1 ratio onto Matrigel- or Laminin-511 E8-coated culture substrates.	human albumin secretion, early hepatic marker genes such as ALB, G6P, HNF4A, and CYP3A7 by PGECS- LBs	-PGECS demonstrated a persistent propensity for differentiation without teratoma development and therapeutic potential for treating fulminant liver failure.	[43]
4	Coll et al	2018	iPSc	Hepatic Stellate cells	BMP4 → 4 days BMP4, FGF1, and FGF3 → 6 From FGF1, FGF3, retinol, and palmitic acid → days 6–8 retinol and palmitic acid → days 8 to 12	In pHSCs and iPSC-HSCs, the gene expression of HSC markers and fibroblast markers was evaluated.	create human PSCs that resemble primary human HSCs in terms of phenotypic and functional characteristics.	[44]
5	Yaqing wang et al	2018	human-induced PSCs (hiPSCs)	liver organoid-on-a-chip system	Combining stem cell biology and microengineering to create a 3D perfusable chip system	Albumin secretion and urea synthesis, Cytochrome P450 enzyme activity Drug toxicity assays	increased expression of endodermal genes (SOX17 and FOXA2) and mature hepatic genes, as well as increased cell viability (ALB and CYP3A4)	[45]
6	Coll et al	2018	iPSc	Hepatic Stellate cells	BMP4 → 4 days BMP4, FGF1, and FGF3 → 6 From FGF1, FGF3, retinol, and palmitic acid → days 6–8 retinol and palmitic acid → days 8 to 12	In pHSCs and iPSC-HSCs, the gene expression of HSC markers and fibroblast markers was evaluated.	create human PSCs that resemble primary human HSCs in terms of phenotypic and functional characteristics.	[44]
7	Seon Ju Mun et al	2019	iPSc	Expandable human hepatic organoid	Over 2D monolayers of mature hepatocytes, 3D spherical structures first developed about 9 to 12 days later.	↓NANOG → LGR5's and the ALB, TTR, CK18, and RBP4 ↑epithelial markers and hepatocyte markers, a bile salt efflux transporter (MRP4), ductal markers (CK19 and SOX9)	Organoids displayed self-renewal and were morphologically identical to epithelial organoids produced from adult liver tissue.	[46]
8	Fenfang wu et al	2019	iPSc	Hepatobiliary organoid	stages I and II (days 1–15) → 25% of mTeSRTM culture medium was added to the hepatic differentiation medium stage III (days 15–45) → 10% cholesterol	the capacity to produce, fat and glycogen, and transform substances such as albumin and urea indocyanine green, as well as the capacity to metabolize drugs (CYP3A4 activity and inducibility);	create in vitro functional hepatobiliary organoids from human-induced pluripotent stem cells without the use of external cells or genetic engineering. iPSC-derived liver organoids (HLOs)	[36]
9	Richards et al	2022	Human iPSCs	Human Liver organoids (HLO)	human iPSCs → liver organoids (HLO)	hepatocyte-specific markers: HNF4a and albumin epithelial marker: cytokeratin 17	exhibited the epithelial marker cytokeratin 17 as well as the hepatocyte-specific markers HNF4a and albumin.	[47]

The use of 3D systems has numerous benefits, including the ability to better sustain cell-to-cell contact, which allows cells to communicate directly with one another and to aggregate on their own to form the organization of the cells in the organ. Most of these techniques used the Matrigel matrix. It is now widely accepted that cells cultured using the 3D method are more similar in architecture to function in living tissue than cells cultured using the 2D technique. One of the causes is the development of cell-to-cell contacts and connections between cells and the extracellular matrix in 3D cultures, whereas these interactions are only possible in 2D cultures in the horizontal plane. Cells in tissues are frequently exposed to stratified concentrations of effector signal molecules, nutrients, and waste products, similar to a 3D culture system where the cells located in the middle of the aggregates or organoids have limited access to the components present in the culture medium. Contrarily, since all

Table 2. Various methods to generate liver organoid from iPSC and coculture with other cells

No	Author	Year	Cell source	Product	Methods	Functional indicator/marker	Result	Reference
1	Asai et al	2017	iPSC + MSC +HUVEC (Human umbilical vein endothelial cell)	Human liver organoid	transwell system; HE-iPSC, MSC, and/or HUVEC	Albumin, alpha-1 antitrypsin (A1AT) and urea	Paracrine-soluble factors secreted by MSCs or HUVECs → induce hepatic differentiation	[35]
2	Takanori Takebe et al	2017	human-iPSC-derived hepatic endoderm (iPSC-HE) cells, bone marrow mesenchymal stem cells and human umbilical cord vein endothelial cells (HUVECs)	By creating an Omni-well-array culture platform for mass manufacturing homogenous and miniature liver buds on a therapeutically significant big scale (>10 ⁶)	The aspect ratio of the microwell array is extraordinarily high.	↑Albumin (ALB) and ↓α-fetoprotein (AFP)	a strict production infrastructure for the supply of multicellular organoids	[48]
3	Goulart et al	2019	iPS-derived hepatoblast (iHep)+ iPS-derived endothelial cells (iEC) + iMSC iHep + Human aortic Endothelial Cells (HAEC) + dental pulp (dpMSC)	Liver organoid	Matrigel diluted 1:1 with EGM-2	Albumin secretion, CYP1A1, CYP1A2, and TDO2, TGF-β, and Wnt	reduced activity of TGF-β and improve albumin secretion and liver function.	[37]
4	Ouchi et al	2019	IPsc + mesenchymal cell	multicellular human liver organoids (HLOs)	Definitive endoderm induction → Colonies of hESC and iPSC were seeded on a Matrigel-coated tissue culture plate HLO induction → Day 6 saw the delicate pipetting of spheroids and associated cells to separate them from the dish.	epithelial marker EpCAM, the Kupffer cell markers CD68, the stellate cell marker CD166/ALCAM and EMR, hepatocyte markers HNF4A, CEIPA, RBP4, and ASGR1, Cytochrome p450 Activity (CYP3A4)	With a continuous cell polarity, the PSC-based HLO approach we have presented naturally engages cells to diversify.	[49]
5	Akbari et al	2019	(iPSC)-derived EpCAM-positive endodermal cells are used in the hepatic organoid (eHEPO) culturing system.	Organoids from EpCAM ⁺ cells	modeled argininosuccinate synthetase (ASS1) mutation-induced citrullinemia type 1, a condition of the urea cycle.	Albumin secretion, CYP3A4 activity, Uptake of low-density lipoprotein (LDL), Glycogen storage function,	eHEPOs can be created in as little as two weeks and grown for a significant amount of time (>16 months) without losing their ability to differentiate into mature hepatocytes. eHEPOs are good limitless cell sources that can be used to quickly and effectively produce functioning hepatic organoids.	[41]

cells in 2D monolayer cultures were in direct contact with the culture medium, they were all exposed to the same concentration of the components present in the medium. To modify cell survival, migration, morphogenesis, differentiation, proliferation, and differentiation, it is discovered that the construction of a microenvironment using 3D approaches is more advantageous physiologically, biochemically, and biomechanically [22, 29].

Monolayer culture, also known as 2D flat culture, has been commonly used in the early stages of drug screening. In addition to modifying the distribution of the different cell types in a regulated way, micropatterned surfaces also offer biochemical signals for both parenchymal and nonparenchymal slopes. Table 5 shows the various comparison between 2D and 3D methods in liver organoids for the last 3 years [58].

Table 3. Various methods to generate liver organoid from iPSC and human Embryonic Stem Cells (hESCs)

No	Author	Year	Cell source	Product	Methods	Functional indicator/marker	Result	Reference
1	Ramli et al	2020	iPSCs and hESCs	hepatic organoids	PSC → PFG → HES → HEPS → HOs (50 days)	Albumin or apolipoprotein B levels (ELISA), CYP3A4 activity, Luciferase, alkaline phosphatase (ALP) assay, gamma-glutamyl transferase (GGT)	Cells in organoids differentiated into hepatocytes and cholangiocytes, which express albumin and cytokeratin 7, Apolipoprotein B, cytochrome P450, and albumin were secreted; markers for cholangiocytes included GGT and ALP activity and secretin-induced proliferation. Cholestasis-inducing medications like troglitazone allowed HOs to demonstrate a functional bile canaliculi system.	[50]
2	Shinozawa et al	2021	Human iPSCs and HESC	Hepatic liver organoids (HLO)	iPSCs → foregut induction → hepatic liver organoids (HLO)	ALB, AFP, cytochrome P (CYP) 450 family 2 subfamily C member 9 (CYP2C9), and CYP7A1, marker of polarity and transporter activities, marker pluripotent, albumin secretion, CYP2C9 analysis	A promising test technique for liver toxicology studies is the liver organoid-based Toxicity Screen, which also has uses in drug screening, chemical optimization, mechanistic research, and precision medicine.	[51]
3	Lee et al	2021	hESC and hiPSCs	3D Spheroid formation hepatic organoids	7 Stage - Definitive endoderm 1 - Definitive endoderm 2 - Ventral foregut - Hepatoblast (HB) - Hepatoblast (HB) expansion - Hepatic maturation I - Hepatic maturation II	PAS staining, albumin and urea secretion, α-fetoprotein (AFP), albumin (ALB), and α-1-antitrypsin (A1AT), EpCAM, CK19, SOX9	Its microwell platform can be used to make hPSC-3D-uniHLC-Ss that can be employed as an imaging-based toxicity screening system to foretell medication hepatotoxicity.	[52]

Translational research challenges the clinical application of liver

One of the more alluring methods for treating people with liver failure is hepatocyte transplantation. This is because liver failure patients' human-induced pluripotent stem cell-derived hepatocyte-like cells (iPS-HLCs), which are anticipated to be used for hepatocyte transplantation, can be created on a massive scale. iPSCs are an excellent source for an *in vitro* model of liver disease, as per various protocols to produce hepatic cells from them. They also represent a significant advancement in the field of liver disease since samples taken from patients during surgery or liver transplantation were once a potential source of primary cells [22, 64].

An extracellular matrix that may induce cell aggregation into 3D structures is necessary for creating organoid livers. Most organoid cultures' compositions, including those of the liver, are challenging to explain, and several variations are the result of cultural adaptation. This is a drawback to its potential use in several therapeutic applications and regenerative medicine. Further effort is required as synthetic platforms develop bioengineering that can aggregate liver cells in a 3D structure without losing their specifications. Another limitation is that the organoid liver is not completely in its entirety and the various types of cells present in the liver and their degree of regularity. The direct clinical application of organoid technology still faces various challenges. The transformation toward malignancy in organoids originating from stem cells is of particular concern after transplanting and thorough animal model observation is a way of dealing with this problem [22].

Finding the best way to produce organoids is another difficult task. Although the current technique for organoid cultivation using an extracellular matrix (Matrigel) and bioengineered factor creation is crucial, it involves components of animal origin (bovine serum). This substance may contaminate organoid products and produce adverse effects on human hosts. The use of bioproducts without chemical explanation has a negative impact, so in the future,

Table 4. Various methods to generate liver organoid from primary cells

No	Author	Year	Cell source	Product	Methods	Functional indicator/marker	Result	Reference
1	Scepers et al	2017	Primary hepatocyte Primary human hepatocytes + fibroblast iPSC	Human liver on a chip model	Cell aggregates were reconstituted in PEG-DA prepolymer, fed into a water-in-oil droplet generator, and continuously polymerized on-chip under a low UV light dose.	HNF4 α , albumin, HNF1 β , CYP1A1, CYP2C9	As iPSC cells differentiated into hepatocytes, they gathered and were encapsulated, producing microtissues that showed induced CYP activity and stable albumin synthesis on a chip.	[53]
2	Gomez-Mariano et al	2020	Ductal cells of the human liver	Liver organoids	Duct isolation \rightarrow liver organoids	albumin (ALB), apolipoprotein B (APOB), apolipoprotein C3 (APOC3), cytochromes CYP3A4, CYP2C8, phospholipase A2 group XIIB (PLA2G12B), UDP glucuronosyltransferase family 2 member B4 (UGT2B4), acyl-CoA thioesterase 12 (ACOT12), insulin-like growth factor 2 receptor (IGF2R), UDP glucuronosyltransferase family 2 member B11 (UGT2B11), 3-hydroxy-3-methylglutaryl-CoA synthase 2 (HMGCS2), transmembrane serine protease 6 (TMPRSS6), aminocarboxymuconate semialdehyde decarboxylase (ACMSD) and coagulation factor XIII B chain (F13B)	The liver organoid model recapitulates the key features of Z-AAT deficiency and provides a useful tool for disease modeling.	[54]
3	Guo et al	2021	Skin fibroblast \rightarrow iPSCs	hepatocyte-like cells (iHep) and Hepatocyte organoids (iHep-Orgs)	Skin fibroblast \rightarrow iPSCs \rightarrow iHep \rightarrow iHep-Orgs	albumin (ALB) and fetal hepatic protein: α -fetoprotein (AFP) immunofluorescens, PAS staining and Dil-Ac-LDL, hepatic genes (ALB, AFP, AAT, CYP3A4), ALB secretion and CYP3A4 activity	Albumin (ALB), and α -fetoprotein (AFP). PAS staining and Dil-Ac-LDL revealed glycogen buildup and LDL uptake in iHep-Orgs. ALB secretion and CYP3A4 are secreted by iHep-Orgs, which have higher levels of hepatic gene expression than iHep and iPSCs.	[55]
4	Hou et al	2022	Hepatocytes were isolated from liver tissues	Liver organoids (LO)	Hepatocytes diff to LO	hepatocyte markers: hepatocyte nuclear factor-4-alpha (HNF4 α), E-cadherin (E-Ca), Zonula occludens-1 (ZO-1), and Cytokeratin 19 (CK19) gene expression of liver maturation genes: ALB, HNF4A, E-Cadherin, ZO-1, KRT19, and CFTR	High expression of maturation markers, such as hepatocyte nuclear factor-4-alpha (HNF4 α), E-cadherin (E-Ca), and albumin, allows organoids to develop into hepatocytes	[56]
5	Tomofuji et al	2022	Mouse intrahepatic bile ducts cells	Mouse liver ductal organoids	intrahepatic bile ducts cells \rightarrow liver ductal organoids	cholangiocyte specific markers \downarrow Krt19, \uparrow Sox9, and \uparrow Cftr in ductal organoids \downarrow the expression of hepatocyte-specific markers: Alb, Hnf4a, and Cyp3a11 was low	A potential cell source for bile ducts from bioengineered liver grafts using three-dimensional scaffolds is liver ductal organoids.	[57]

bioengineering techniques are necessary to produce organoids using methods that can be explained chemically [65].

Determining the proper cell type and creating vascular tissue that will enable cell aggregation provide significant challenges for organ bioengineering. The determination of celltypes, ideal cell volume, and seeding techniques are the major challenges in producing vital liver functions. To better understand how liver cells may organize themselves to produce the liver, one of the body's most complicated organs, these fascinating difficulties call for a multidisciplinary approach combining biologists, doctors, and bioengineers [7].

Table 5. Various comparisons of 2D and 3D methods in liver organoids

No	Comparison	Cell source	Methods	Result	References
1	2D	hiPSC	synthetic hydrogels poly (ethylene glycol) (PEG) hydrogels	Significantly less fetal liver-associated α -fetoprotein was secreted by hPSC-HEPS in 3D cultures compared with 2D cultures, indicating greater differentiation.	[59]
	3D		encapsulation gelatin-coated cell culture dishes		
2	2D	hepatocellular carcinoma cell line HepG2, HUVECs, and MSCs	Perfusion and nonperfusion methods using tube pump	Culture dimensionality has a significant impact on gene expression profiles.	[60]
	3D		methods using tube pump		
3	2D	Primary hepatocytes from mice liver	Culture dish	For up to 7 days, the 3D hepatic architecture showed greater expression levels of functioning hepatic genes and proteins.	[61]
	3D		cell-alginate 3D bio-printing technique		
4	2D	Peripheral blood-derived human-induced pluripotent stem cells (hiPSCs)	cell culture plate coated Matrigel	The liver organoids' hepatocytes were more mature, as evidenced by the fact that they synthesized ALB higher than that of the 2D culture but with low expression of endoderm-specific SOX17.	[62]
	3D		3D culture using a mixture of Matrigel		
5	2D	HeparG cell line	monolayer	Compared with 2D cultures, 3D cultures were more vulnerable to the mitochondrial damage caused by acetaminophen.	[63]
	3D		spheroid formation with pulverized liver biomatrix scaffolds (LBSs)		

In recent years, organoid 3D cultures of various tumor subtypes and organs have been successfully developed, paving the way for tumor research. Organoid 3D culture is used to explain tumor diversity, to model cancer in the lab, and to determine response to therapy. A promising strategy to combat drug resistance and improve the effectiveness of tailored anticancer therapies is creating a biobank and creating a next-generation matrix [3].

Although the current progress is very significant, there are still unmet clinical needs. This encourages the development of alternative treatments for diseases and impaired liver function. A critical issue that has yet to be resolved is how to accelerate the translation of cell therapy into clinical practice, which is a prerequisite for liver transplant recipients to increase engraftment and proliferation of donor cells, and the development of noninvasive and tracking methods to monitor accurate cell survival and processes [66].

Regenerative medicine for the human liver has seen numerous significant advancements. This includes the development of a replicable cell source and the prospect of overcoming low donor organ and hepatocyte stability, which is an immune system challenge. Although there have been many developments, liver cells derived from stem cells require further development before they can be used clinically [67]. An interesting future is offered in this research because efforts now focus on ways to enhance cell activity, engraftment, and

stability. Deeper research has been conducted on alternative medicines, xeno-organ, scaffold-based, and specific cell transplantation. Hepatocytes and MSCs have been used in cell transplantation alone in clinical settings. Xeno-organ and cell transplantation are combined in a thorough procedure known as scaffold-based transplantation. Clinical applications of scaffold-based transplantation will be the subject of future study [68].

For regenerative medicine to be successful, hiPSC-based LO must be safe *in vivo*. Consequently, reliable genome editing techniques, effective *in vivo* delivery methods, and the usage of xeno-free materials are all required. Genetic and epigenetic stability must be examined when the iPSC-based liver organoid is being created and grown. The current difficulties in disease modeling and medication development are to increase complexity, decrease heterogeneity, and improve maturity [69]. Another crucial area for future research is the well-known risk of teratoma development because of undifferentiated cell contamination following cell transplantation. Procedures that may remove nondifferentiated cells from a batch of samples created using differentiation processes must be set up before being used in a clinical context [70].

Conclusion

This review summarized alternative protocols to differentiate hepatocytes from iPSC and to generate LO based on iPSC from varying perspectives. For the growth of human iPSC cells to LO, numerous procedures have been created. Future studies are still anticipated to focus on the clinical use of LO in ESLD patients.

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